

RESEARCH ARTICLE

Design of a wireless measurement system for use in wireless power transfer applications for implants

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The performance of wireless power transfer (WPT) systems is a function of many parameters such as resonance matching, coil quality factor, system impedance match, and others. When designing and testing WPT systems, reliable measurement of system performance is essential. In our application, we use WPT to power biomedical implants for telemetry acquisition from small rodents, where rodent behavior data is used to study disease models. Such an application employs a large primary coil and a much smaller moving secondary coil, which can be defined as a loosely coupled WPT (LCWPT) system. This paper presents a novel wireless measurement system (WMS) that is used to collect real-time performance data from the secondary circuit (implant), while testing LCWPT systems. Presently, measuring the performance of the secondary side of LCWPT systems while they are in operation can be problematic. The literature reports various measurement errors when using voltage/current probes, or coaxial cables placed directly into the primary magnetic field. We have designed the WMS to greatly reduce such measurement errors, where the WMS measures the induced voltage (and hence received power) and relays this information by radio. Experiments were done to test the WMS, as well as comparison with cable-based measurements.

Keywords: Loosely coupled wireless power transfer, Magnetic resonance, Parameter measurement, Design, Biomedical telemetry device

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1. INTRODUCTION

Wireless power transfer (WPT) is used in various biomedical applications to power telemetric devices and implants. It can be used to supply power to implanted telemetric devices for indefinite periods, without the need for batteries, battery replacement surgery, or transcutaneous wiring. There are many designs of WPT systems that have been proposed, where power requirements for implantable devices vary with the application and can range from a few milliwatts to dozens of milliwatts [1–3].

Reliable measurement of system performance is needed for designing and testing WPT systems. This requires the use of a measurement system to collect real-time performance data from the implant (secondary coil circuit) in a way that does not interfere with the device performance.

Our work involves a telemetric device called the rodent implant device (RID) for a freely moving small rodent. It is suitable for subcutaneous implantation in a rat, and is suitable as a head-mounted device for a mouse. Figure 1 illustrates the

concept for telemetry acquisition, where the RID is located on the head of a freely moving rodent within a small housing cage, around which the primary coil is wrapped.

A characteristic of WPT applications for rodent telemetry acquisition is the loose coupling between the primary and secondary coils, providing low levels of power transfer [2]. Our work involves such loosely coupled WPT (LCWPT) where we employ a large primary coil to transmit power to a much smaller secondary coil (implant) that is in motion. To compensate for loose coupling, the use of resonant circuit systems is employed to create boosted voltage/current levels at the secondary coil, even in the presence of low coupling coefficients [2, 4].

In order to characterize LCWPT systems, some key performance parameters need to be accurately measured/obtained at the secondary circuit. These include the induced voltage, the received power, and the overall efficiency of the LCWPT system. Presently, measuring the performance of the secondary side of LCWPT systems while they are in operation can be problematic when using voltage/current probes, or coaxial cables placed directly into the primary magnetic field. A number of researchers have measured the induced voltage, the received power, or the efficiency of WPT systems with various schemes using coaxial cables, twisted-pair cables, or oscilloscope voltage/current probes. Jow *et al.* used a digital oscilloscope (MSO4034B, Tektronix) to measure the peak-to-peak voltage across the LC-tank that

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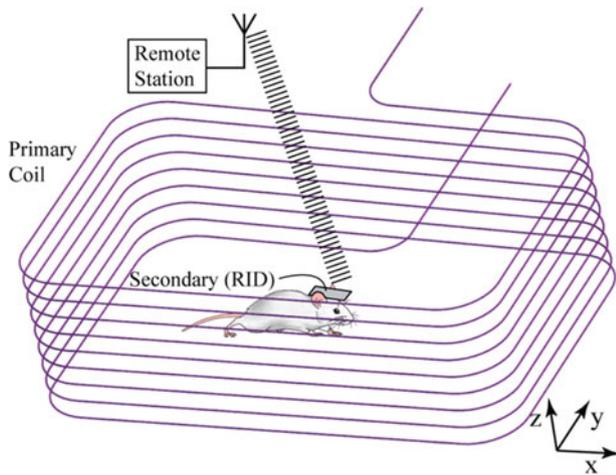


Fig. 1. Small rodent WPT concept, with primary coil wrapped around a small mouse housing cage sized $300 \times 190 \times 120 \text{ mm}^3$ (length \times width \times height).

was connected to a 500Ω resistor load, in their secondary circuit. To do this, they placed a voltage probe within the primary coil's electromagnetic field, to measure the induced voltage in the secondary LC-tank circuit, and they calculated the received power [5]. Pinuela *et al.* initially measured the induced current of their secondary using an Agilent N2783A current probe. However, they noted that the results did not reflect the true of operation of their WPT, as current probes are not capable of measuring the induced current precisely in the presence of significant electromagnetic noise. Also, they could not measure the induced voltage (V_{ind}) using a voltage probe across the load, because the capacitance of the probe can detune the resonance of the receiver circuit. Therefore, they measured the efficiency of their WPT system using a thermal measurement scheme. This was done by measuring the temperature of the heat sink of the receiver coil, and the temperature of their metal film resistor load, by calculating the applied DC input power to their WPT system [6]. Russell *et al.* placed the resistor load of their secondary outside the primary field of their WPT system, and connected that load to the secondary coil via twisted-pair wires. They measured the DC voltage across the resistor load using a NI card (PCI-6025E) interfaced with LabVIEW [7]. Zhao *et al.* built a LCWPT system for an epiretinal prosthesis application. They measured the induced voltage by connecting a voltage probe and a ground probe across the resistor load of the secondary circuit, all of which were within the primary coil's electromagnetic field. These probes were part of a single coaxial cable, which was connected to an oscilloscope [8]. Xu *et al.* built a WPT system for rodent (rat) applications, where their WPT system was based on four coils: driver coil, transmitter coil, receiver coil (secondary coil), and load coil (application load). Their load coil is intended for implantation subcutaneously within the dorsal region of a rat. They likely used a coaxial cable to connect their load coil to an oscilloscope, to measure the peak-to-peak induced voltage of the load coil [9, 10]. Dionigi *et al.* presented a secondary resonator based on a coaxial cable, which is suitable for WPT applications [11, 12]. His work indicates that coaxial cables can affect the magnetic resonance of WPT systems.

In this work, we designed, constructed, and tested the wireless measurement system (WMS) to avoid potential measurement errors inherent with coaxial cables, twisted-pair cables,

or oscilloscope probes within the primary field. The WMS is connected across the secondary load, R_L of the RID to measure the induced voltage received, as shown in Fig. 3 for our LCWPT system.

This paper is organized as follows. Section I shows the research motivation for the WMS system, and other measurement systems. Section II illustrates the methodology of this work. Section III describes WPT theory. Section IV shows the WMS design for WPT system. The experimental setup is described in Section V. The experimental results are reported in Section VI. A discussion of the results is provided in Section VII. Finally, the conclusion is in Section VIII.

II. DESIGN METHODOLOGY

There are a few possible ways to measure the power transfer of LCWPT systems. These include: (i) using current probes to measure the current passing through the secondary load, R_L , while it is within the primary electromagnetic field. (ii) Using voltage probes to measure the voltage across the secondary load, R_L , while it is within the primary field. (iii) Placing the secondary load, R_L , outside the primary field and connecting it to the secondary coil via coaxial cable or twisted-pair wires. Then, measuring the current/voltage of the load R_L with oscilloscope probes.

In regards to approach (i) or (ii), Pinuela *et al.* found that a probe's capacitance of 15 pF was enough to detune the secondary coil from resonance. They also concluded that current probes were not capable of measuring the current accurately in the presence of significant electromagnetic fields [6] due to noise. Hence, oscilloscope probes should not be used inside the primary field electromagnetic zone.

In regards to approach (iii), coaxial cables or twisted-pair cables can be used to spatially move the load R_L farther away from the primary field, allowing measurement of the voltage across the load, or the current through the load, as Russell did in [7]. However, twisted/coaxial cables add an impedance to the secondary circuit. For example, coaxial cable has an impedance of 50 or 75 Ω depending on connector type. This impedance increase may cause impedance mismatch, leading to reflected power loss in the secondary coil.

The purpose of this work is to measure the power transfer of LCWPT systems precisely using a cable-free (wireless) approach. By avoiding the use of coaxial cables, twisted-pair wires and current/voltage probes, we are able to avoid the problems described above. The design of the WMS is explained in Section IV.

We used the WMS to measure the received power using two different experimental telemetric devices: (1) a secondary coil called the *air core*, which consists of a simple coil wrapped around a small printed circuit board (PCB) [2]. (2) A variation of the *air core* employing ferrite rods, where four ferrite rods are placed at the corners of the PCB within the secondary coil. This configuration is denoted as the four medium ferrites (4MF). We designed and built it to improve the coupling, as explained in [2].

III. WPT THEORY

Electromagnetic inductive power transfer systems operate on the principle of changing magnetic fields to create alternating

currents through a primary coil that induces a voltage onto a secondary coil. By Faraday’s law, the resulting induced voltage (V_{ind}) at the secondary coil when it is parallel to the primary coil, is given as [2, 13]:

$$V_{ind} = -\frac{N_p N_s \mu_0 \mu_r A_S a_p^2}{2(\sqrt{a_p^2 + r^2})^3} \cdot j\omega I_p, \tag{1}$$

where I_p is the current applied to the primary coil, N_p is the number of primary turns, a_p is the primary coil radius, N_s is the number of secondary turns, A_S is the loop area of the secondary coil, μ_0 is the permeability of free space, ω is the angular frequency, μ_r is the relative permeability of a specific medium, and r is the transmission distance, where r is calculated as $\lambda/2\pi$, where λ is the electromagnetic wavelength.

The coupling coefficient is defined as a dimensionless value that characterizes the relation between two coils (primary and secondary). For LCWPT biomedical telemetry devices, this coefficient is between 0.1 and 10%, and may vary due to coil-to-coil separation distance, coil-to-coil diameter ratio, coil-to-coil angular orientation, and other factors [2, 14–16]. The low coupling coefficient of many LCWPT systems leads to poor power transfer. Therefore, nearly all WPT systems use magnetic resonant coupling between the primary and secondary coils, to increase the efficiency [9]. Tesla first proposed the magnetic resonant technique [17]. In our work, we measure overall efficiency as: (received power on the RID/DC power supplied to the primary circuit) [2].

There are four topologies for achieving magnetic resonant coupling between the primary and secondary coils. The topologies are SS, SP, PP, and PS for WPT systems, where the first S or P stands for series or parallel compensation of the primary winding, and the second S or P stands for series or parallel compensation of the secondary winding. In this work, the PP topology is used, as shown in Fig. 2.

At magnetic resonance, the reactive components cancel and the impedance is simply the real component, which is the resistive loss of the secondary tank. To achieve maximum power transfer to the load, it is recommended to use the optimum load resistance (R_L), as explained in detail in [2]. The maximum transferred power via the inductive link is defined as [18, 19]:

$$P_o = \frac{V_{ind}^2}{R_L}. \tag{2}$$

IV. WMS DESIGN FOR WPT SYSTEMS

The main motivation for the WMS is to measure the power transfer of our LCWPT system. Given this goal, a set of design requirements for the WMS are established, and summarized in Table 1.

Several design iterations were undertaken to create the WMS, to meet the design requirements and to achieve a robust measuring system. A high-level diagram of the WMS connected to the RID is provided in Fig. 3. The requirement to minimize volume keeps the WMS compact and lightweight. It also minimizes physical interference when connected to the RID, and allows for easy placement and orientation within the primary coil. Ideally, the WMS should not disturb the primary

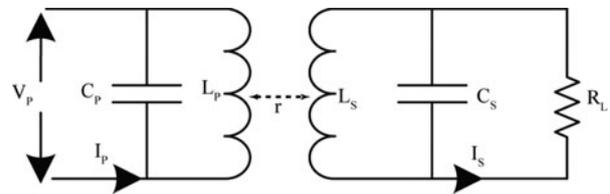


Fig. 2. PP topology of primary and secondary coils.

Table 1. Design requirements for the WMS.

Design requirement	Description	Value/range (units)
Maximum volume	Max volume of WMS	1600 (mm ³)
Non-disruptive to induced field	WMS design should not interfere with resonance or coupling of the WPT	-
Measure induced voltage	Wide measurement range across the secondary load	0–63 (V)
Wireless data transmission	Transfer the measurement data by radio signal	4800 bits/s
Self-powered	Powered by lithium-polymer battery	4.2 (V)
Disconnectable	WMS should be easily removable	two header connector

magnetic field, and should not have a significant effect on the system coupling. As noted in the methodology, a wireless (radio link) communication system has been designed into the WMS to transmit the measured data to an external base-station that records it. The WMS has an on-board microcontroller, a radio, and other electronics requiring power, which is supplied by a battery. This is needed since the WMS must operate independently of the WPT system, which it measures.

Several detailed design notes are provided here regarding the physical construction of the WMS: (i) we used the Nordic nRF24LE1-F16Q24 system on-a-chip (SOC) with embedded microcontroller and radio, since it is a low-power design suitable for RF applications [20]. (ii) The WMS was designed as a four layers PCB that includes power (V_{CC}) and ground planes in the middle, and two routing planes (top and bottom), for best performance in RF applications [21]. (iii) We used surface-mount devices (SMD) of size 0201/0402, since these sizes improve the RF performance and have good thermal properties [22, 23]. (iv) We built a customized impedance matching circuit network for the RF

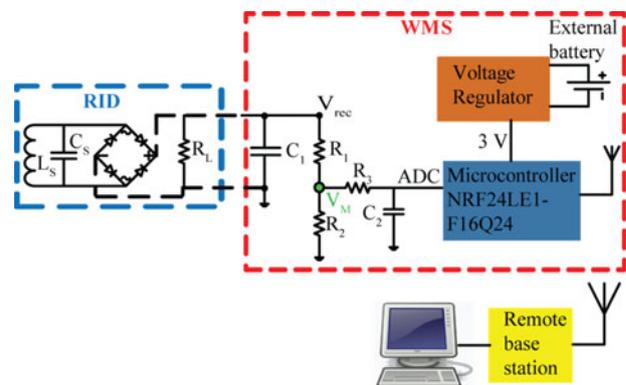


Fig. 3. High-level diagram of the WMS configuration.

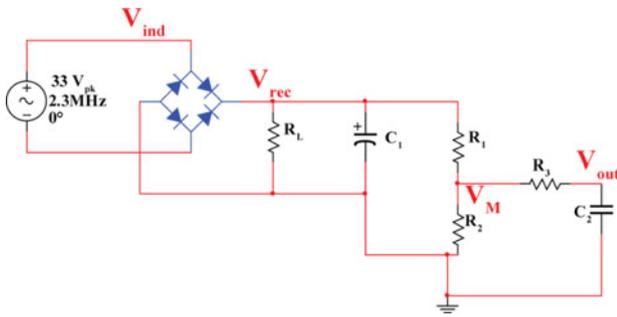


Fig. 4. Multisim model of the RID connected to the WMS.

antenna (FR05-S1-N-0-110) [24], by following the schematic circuit diagram of the QFN24 as described in [20]. (v) We avoided use of nonlinear components (such as voltage regulators or zener diodes) in the measurement stream. These components may affect the resonant frequency of the secondary circuit, as mentioned in [25]. (vi) We used a lithium-polymer (non-metallic) battery to power the WMS, since it is small and its composition is minimally disruptive to the primary field, which avoids the problems described in point (v). We cannot use induced power from the RID to power the WMS, since that power is variable during development experiments.

The design of the measurement circuit on the WMS is described here. The WMS measures the voltage developed across R_L on the RID, which represents the application load. The value of R_L is pre-selected to ensure a good impedance match with the $L_S C_S$ tank and rectifier of the RID.

The WMS employs a voltage divider when making measurements. This is needed since the voltage (V_M) measured by the microcontroller cannot exceed the internal reference value of the analog-to-digital converter (ADC). The reference value is set by an internal bandgap of the microcontroller (nRF24LE1), which is nominally 1.2 V [20]. The system was simulated with Multisim software (National Instruments) to configure the resistor and capacitor values. Figure 4 shows the Multisim model with voltage labels for the simulation results. The voltage source represents the induced voltage (V_{ind}) from the $L_S C_S$ tank of the RID. The maximum received voltage within the $L_S C_S$ tank of the *air core* configuration is 66 V (peak-to-peak), assuming a secondary load R_L of 5 kΩ, and the parameter values as listed in Table 2 (smoothing capacitor, voltage divider and filter). The voltage points at V_{rec} , V_M , and V_{out} of the WMS simulation are plotted in Fig. 5, where V_{rec} is 31.5 V, and V_{out} reaches value V_M after 90 μs. By using equation (3) with the parameter values of the

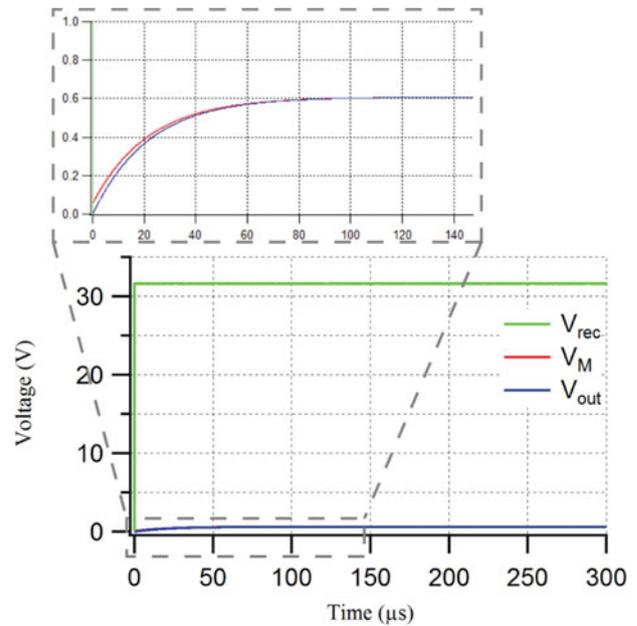


Fig. 5. Voltage traces of the WMS simulation.

voltage divider and the filter, V_M is found to be 0.608 V, which corresponds to Fig. 5.

The measured voltage (V_M) is digitized using a 12-bit setting on the ADC relative to the internal reference value of 1.2 V. With values of the voltage divider resistors R_1 & R_2 as shown in Table 2, the WMS is able to measure DC (V_{rec}) voltages up to 62.4 V. By changing voltage divider resistors R_1 & R_2 , different measurement resolution and ranges are possible, as explained in equation (3). We can ignore the voltage drop over the filter (R_3 & C_2), as the resistance value of R_3 is small compared with R_2 , as shown in Table 2. We can back-calculate the rectified voltage (V_{rec}) over the resistor load R_L as follows:

$$V_M = V_{rec} \frac{R_2}{R_1 + R_2},$$

$$V_{rec} = V_M \times \frac{R_1 + R_2}{R_2},$$

$$V_{rec} = \frac{V_{A/D}}{2^{12} - 1} \times V_{Ref} \times G, \tag{3}$$

where

$$V_M = \frac{V_{A/D}}{4095} \times V_{Ref};$$

G: Voltage divider factor ($R_1 + R_2/R_2$), it is 52;
 V_{ref} : Internal reference (1.2 V).

The WMS is based upon a SOC from Nordic Semiconductor (SOC model nRF24LE1). This SOC includes a 2.4 GHz RF transceiver, an 8-bit microcontroller, embedded Flash memory (16 kB), and a set of on-chip analog and digital peripherals [20]. The WMS circuit schematic was designed using Altium CAD software, where the values of the electronic components (R , L , and C) are provided in the diagram of Fig. 6.

Table 2. Final design parameters for the WMS.

Design parameter	Description	Design value (units)
Overall size	$L \times W \times H$	$35 \times 18 \times 1$ (mm ³)
Weight	The weight of the WMS only	3 (g)
C_1	Smoothing capacitor	0.1 μF
R_3 & C_2	Filter	1 kΩ & 2 nF
R_1 & R_2	Voltage divider resistor	510 & 10 kΩ
Nonlinear component	Power the voltage regulator externally	-

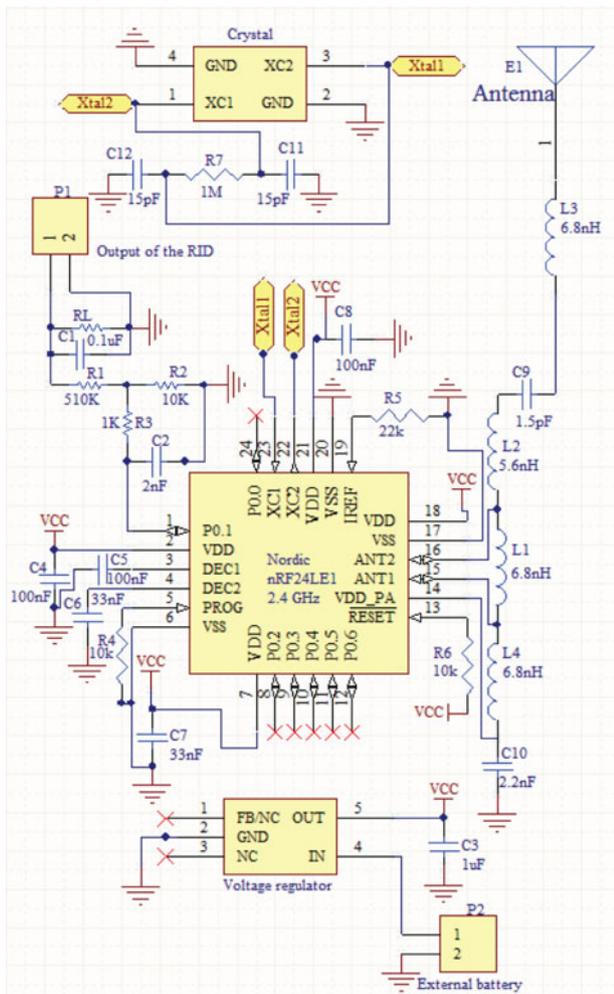


Fig. 6. Schematic diagram of the WMS.

The radio communication protocol is built into the Nordic platform, and uses a proprietary handshaking network protocol to transfer voltage data (V_M) in digital format. The communication frequency between the WMS and the base station is 2.4 GHz. For this application data were sampled and transmitted at an effective rate of 29 Hz. The transmitted data/packets are displayed and saved using a custom graphic user interface. The transmission range of the Nordic RF system is approximately 6 m, which is adequate for this application.

The microcontroller chip on the WMS is programmed by initially compiling the bootloader program on a computer, and then downloading it to the chip using a USB-connected interface board. The bootloader program is subsequently used to wirelessly upload program code using the base station. We use Keil μ Vision4 as a program debugging software that compiles the code and generates its hex file. Then the generated hex file is uploaded onto the microcontroller chip wirelessly.

V. WMS EXPERIMENTAL SETUP

Our LCWPT system can be divided into two parts, namely the primary circuit and the secondary circuit, as illustrated in

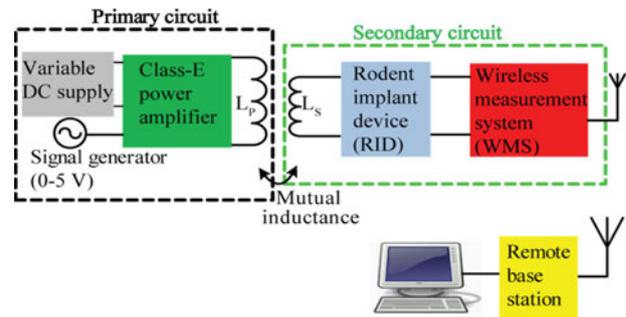


Fig. 7. Block diagram of LCWPT system with the WMS.

Fig. 7. The WMS design was tested with two different RID configurations (*air core* and 4MF). Magnetic resonant coupling is achieved by tuning the parameters of the primary and secondary circuits such that both resonate at the same frequency.

Power is supplied to the primary circuit using a DC power supply. A signal generator (Agilent 33250A) provides a driver signal to a Class-E power amplifier, which is used to generate sinusoidal current (I_p) in the primary coil (L_p). The alternating electromagnetic field in the primary coil induces a sinusoidal voltage (V_{ind}) in the secondary coil (L_s). The induced voltage is rectified within the RID into a DC voltage (V_{rec}) that provides power to the application load (R_L). The V_{rec} is measured across the load R_L using the WMS as explained in Section IV.

A switching inverter is used to supply the primary coil (L_p) with sinusoidal AC current. There are many designs for power amplifier inverter circuits, categorized in Classes C, D, and E. We used the Class-E amplifier design to drive our primary coil, since it is a common approach that is used extensively. Sokal *et al.* demonstrated the operational characteristics of their zero-voltage-switching inverter (ZVS) [26] using this approach. The Class-E is the preferred topology as it has high power efficiency, and it minimizes the stress on the switching element. The parallel capacitance normally present in a Class-E amplifier has been replaced here by a diode where the diode allows for suboptimum operation. The antiparallel diode in the MOSFET turns on when the voltage crosses zero voltage, before the oscillation waveform reaches its minimum. This regime is referred to as suboptimum operation [27].

Our Class-E amplifier is configured as parallel resonance, where C_4 works in combination with C_{tank} to create a parallel primary resonant tank, as shown in Fig. 8. We vary C_4 to adjust the resonance of the primary circuit. The series

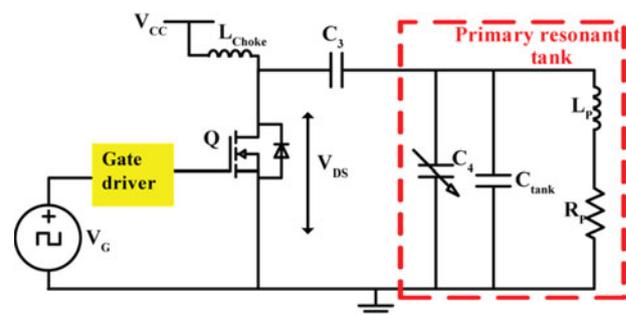


Fig. 8. Class-E amplifier (parallel resonance with C_{tank} and L_p).

capacitor (C_3) shields the MOSFET from the high voltage developed by the primary resonant tank [27]. A pulse train (V_G , duty cycle 0.5) is applied at the gate driver (MIC4421). The switch used is a MOSFET (STP16NK65Z) with high power handling and nanosecond switching capabilities [28, 29]. This MOSFET was also selected due to its relatively low output capacitance (C_{oss}) at high V_{DS} [30]. It is important to note that C_{oss} is effectively absorbed by C_4 [6].

For increasing the WPT efficiency, tuning peak-to-peak voltage is just as important as switching at zero-voltage-zero-current. Identification of the ideal voltage and current waveforms that minimize switching losses, led to the design of Class-E ZVS power amplifiers by Sokal *et al.* [26, 30, 31]. Our power amplifier is designed to deliver a maximum sinusoidal current (peak-to-peak) of up to 7 A through the primary coil. This can generate sinusoidal voltages (peak-to-peak) of up to 2.3 kV across the primary resonant tank.

The RID has an $L_S C_S$ tank and a full bridge rectifier, as shown in Fig. 9, for both the *air core* and 4MF configurations. The rectification is an important part of the secondary coil in a WPT system, where it is vital to efficiently utilize the generated V_{ind} [32]. High frequency rectifiers have two loss contributions associated with the diodes; losses due to forward conduction and a high frequency loss that can be attributed to the finite switching time of the diode. The switching losses occur as a consequence of the reverse recovery time of the diode. The forward conduction losses exist due to the forward voltage of the diode and the loss associated with its non-zero series resistance. Several rectifier topologies can be implemented for LCWPT (low power applications). The small diameter of the secondary coil (L_S) and the poor coupling coefficient, make it difficult in most applications to induce a high secondary voltage (V_{ind}). For this reason, full-bridge rectifiers with quad diodes designed for use in ultra-high-speed switching applications [33] are preferred to rectify the induced voltage (V_{ind}) [25].

To achieve high quality factors, inductors with low effective series resistance (ESR) are required for high frequency operation, due to the skin effect and proximity effect. To reduce the ESR, multistrand Litz wires are commonly used [15, 34]. For implant applications, the preferred frequency range of operation is from 100 kHz to 4 MHz, where minimal biological effects have been reported, in contrast to the extreme-low-frequency band and the microwave band [35]. In this work, the two RID configurations employ 48 AWG

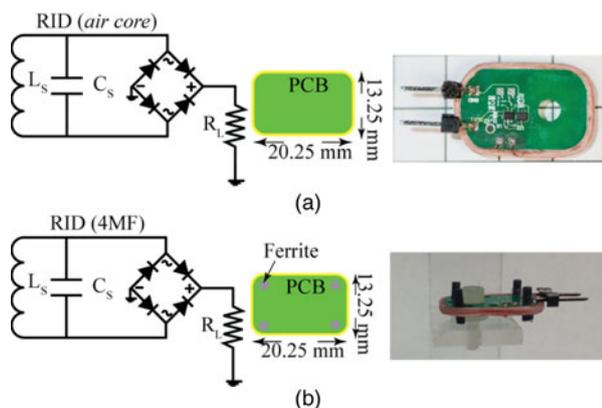


Fig. 9. RID configurations; (a) *air core*, (b) 4MF.

Table 3. Parameters of the secondary coil of the RID configurations.

Configuration	Q	L (μH)
<i>Air core</i>	36	22.4
4MF	44	29.5

Table 4. Measured resonant frequency and the impedance magnitude of RID configurations.

Configuration	F_{res} (MHz)	R_{LC} (k Ω)
<i>Air core</i>	2.302	10.1
4MF	2.057	12

Litz wire. The number of turns used in the *air core* and 4MF configurations is 28 turns (7 turns per layer, 4 layers). The resonant frequency of each RID configuration is a function of its own $L_S C_S$ tank properties and is not adjustable. The $L_S C_S$ tank employs a fixed 235 pF capacitor (C_s) for all configurations. The coil parameters (Q and L_s) of each configuration are listed in Table 3, as measured using a HP 4285A LCR meter. A HP 4193A vector impedance meter is used to measure the resonant frequency and impedance of the $L_S C_S$ tank of each RID, as listed in Table 4.

The impedance match within the RID must be appropriate to minimize internally reflected power loss between the $L_S C_S$ tank and the secondary load R_L . When considering this impedance match, the reactive part (capacitive component) of full-bridge impedance is considered part of the $L_S C_S$ tank impedance [2].

The primary coil is wrapped around an animal cage sized $30 \times 19 \times 12 \text{ cm}^3$ (length \times width \times height). To mimic various angular orientations of a rodent, four experimental fixtures were constructed to hold the RID at various orientations, which are 0° , 30° , 60° , and 90° . These angles are with respect to the x - y plane and the longitudinal axis of the primary coil, as shown in Fig. 1. Each fixture holds the RID at a 3 cm height above the base of the cage, and is located in the center of the cage. Figure 10 shows the experimental setup of the complete WPT system. The output voltage of

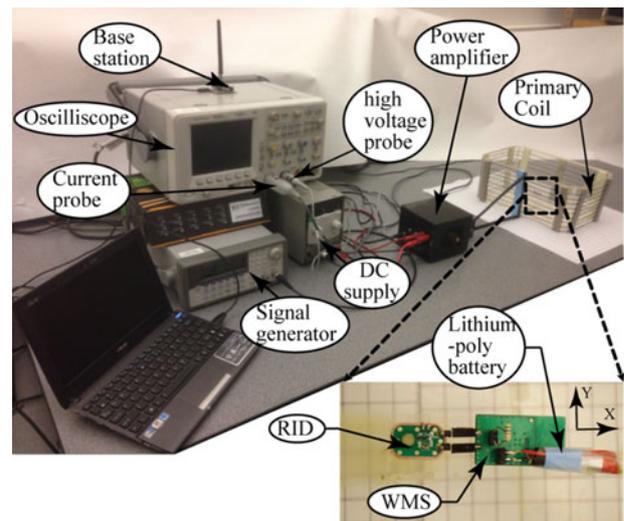


Fig. 10. WPT experimental setup.

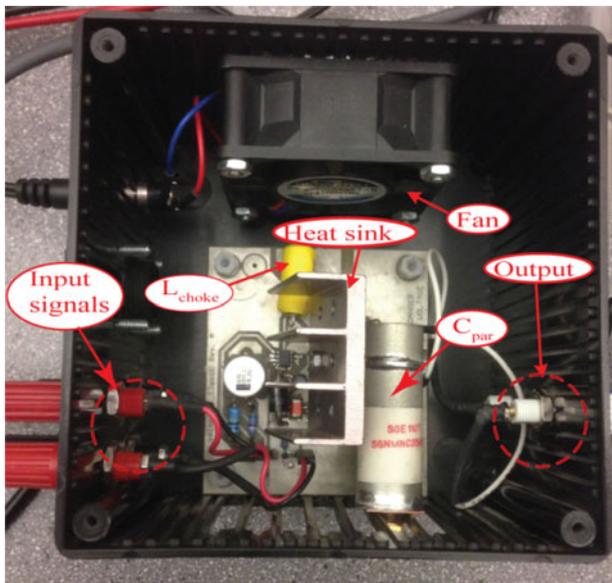


Fig. 11. Top view of the Class-E power amplifier.

the Class-E power amplifier is measured by a high voltage probe, and the primary current (I_p) is measured by a current probe (Agilent N2893A). The high voltage and current probes are connected to the oscilloscope. Prior to each WPT experiment, a calibration procedure is performed to ensure the magnetic resonant coupling is achieved between the primary and secondary circuits. This is done by verifying (re-measuring) the RID properties, and matching the resonant frequency of the system by tuning the primary circuits. The primary circuit is tuned by adjusting the signal generator frequency and adjusting the variable capacitor (C_v) in the Class-E power amplifier.

Most of the system losses occur as heat at either the amplifier transistor (MOSFET) or the primary coil (L_p). A temperature increase at the primary coil (L_p) is not critical because it is a passive component and more resilient to heat [25]. A 12 V DC brushless fan is used to achieve an air flow for forced air cooling. In addition, the heat sink on the MOSFET further enhances the heat-dissipation capabilities. Figure 11 shows the top view of the Class-E power amplifier.

The magnetic resonant properties of our LCWPT system were evaluated with and without the WMS attached. This was done by first measuring the resonant frequency of the RID $L_S C_S$ tank, as listed in Table 4. The resonant frequency of 4MF was 2.057 MHz, when we measured the resonant frequency of the RID alone (without connecting the WMS). When we measured the resonant frequency of the RID with the WMS attached, we observed a resonant frequency 2.067 MHz with the 4MF configuration. This difference of frequency is only 10 kHz (0.5%), which shows that the WMS does not cause a large shift in the resonant properties for LCWPT systems.

VI. WMS EXPERIMENTAL RESULTS

The WMS was constructed and a set of experiments was conducted to test its performance. First, we examine the effect of measuring the rectified voltage (V_{rec}) across the secondary

Table 5. Measured voltage V_{rec} and received power P (mW) of *air core* using WMS and the four shapes of the coaxial cable.

Measuring approach		Day 1	Day 2	Day 3	Day 4
WMS	V_{rec}	17.06	17.03	17.06	17.03
	P (mW)	58.2	58.04	58.2	58.04
Straight coaxial cable	V_{rec}	18.7	18.3	17.85	18.02
	P (mW)	69.9	65.7	63.72	64.9
45° tilted coaxial cable	V_{rec}	18.03	17.52	17.2	17.3
	P (mW)	65.1	61.4	59.2	59.9
S-shaped coaxial cable	V_{rec}	21.3	20.2	18.9	19.1
	P (mW)	90.73	81.6	71.5	72.9
Circle-shaped coaxial cable	V_{rec}	21.8	21.1	19.5	20.02
	P (mW)	95	89	76.1	80.2

load (R_L) using the WMS, and compared it with measurements using a physically connected coaxial cable. The measurements using the coaxial cable were performed with one end of the cable connected to the output of the rectifier on the RID, and then running the remaining length of the coaxial cable outside the primary coil. The outside end of the coaxial cable was connected to the load resistor (R_L), where the rectified voltage (V_{rec}) was measured using the voltage probe (measured outside the primary coil since the R_L resistor cannot reside on the RID if using direct cable-based probes). We varied the shape and orientation of the coaxial cable within the primary magnetic field using four shapes/orientations which were: straight cable (parallel to magnetic field), 45° tilted cable (45° to magnetic field), S-shaped bent cable (in plane parallel to magnetic field), and circle-shaped bent cable (in plane parallel to magnetic field). Table 5 summarizes the measured voltage and the received power using both the WMS and the four coaxial cable configurations. All tests were done using the *air core* RID over 4 days, placed at the center of the cage, using a 2.5 A current (sinusoidal, peak-to-peak) applied to the primary coil. We observed that the measured value of the rectified voltage (V_{rec}) using the four shapes of the coaxial cable was not consistent from shape to shape, and also not consistent from day to day. The primary coil (cage), the power amplifier, the oscilloscope, current probe, the signal generator, and the base station remained in the same place each day. However, the secondary circuit (RID), the voltage probe, and the four shapes of the coaxial cable were set up at the beginning of the experiment each day, and taken down at the end of the experiment each day. The measured values from the WMS were very consistent from day to day. The measured values of V_{rec} using the four shapes of the coaxial cable were higher than the values obtained using the WMS by 5–28%.

Another type of experiment was conducted to demonstrate the performance of the WMS, and to compare the WMS to the coaxial cable. To do this, we measured the rectified voltage (V_{rec}) received by the RID, at 13 different locations within the cage field. In one case we used the S-shaped coaxial cable, and in the other case the WMS, to measure V_{rec} . Figure 12 shows a map of these 13 points with their coordinates (x , y). This experiment used the 4MF configuration, a secondary load (R_L) of 10 k Ω , and 2.5 A (peak-to-peak) applied to the primary coil. Figure 13 shows contour plots of V_{rec} measurements on two different days using both the WMS and the S-shaped coaxial cable. As before, the system was set up and taken down each day. Figures 13(a) and

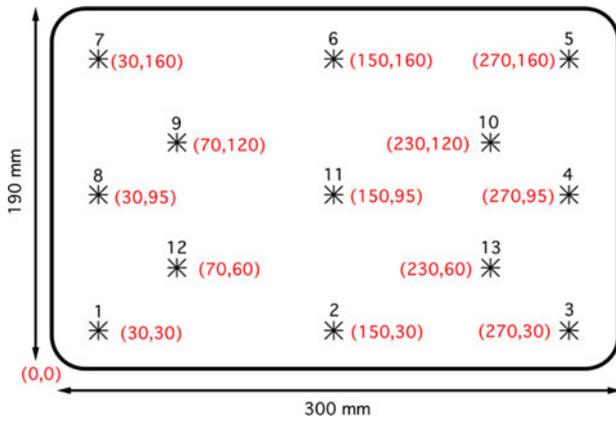


Fig. 12. Top view of the cage showing the locations of the 13 points.

13(b) show the consistency in the measurements using the WMS, based on the relative symmetry of the contour shape (about the horizontal and vertical) and the measurement magnitude (color and contour labels). Figures 13(c) and 13(d) show less consistent measurements using the S-shaped coaxial cable given less symmetrical shape, and less consistency from day to day. Table 6 lists the V_{rec} measurements of the WMS and the S-shaped coaxial cable on Day 1 and Day 2. Two important observations can be made: The variation from day to day of the WMS measurements at similar points, is within 0.11–0.86%. However, the measurements from day to day of the S-shaped coaxial cable at similar points vary from 1.81 to 6.69%. The second observation concerns the expected values themselves. Notice that the 13 points are symmetrically distributed (horizontal and vertical) within the cage. According to theory and computer simulations in reference [2], the field intensity at points 1, 3, 5, and 7 should be the same. As well, the field intensity at points 9, 10, 12, and 13 should be the same. Looking at Table 6, for measured points 1, 3, 5, and 7, we can see the WMS values are within 0.90%, and for measured points 9, 10, 12, and 13 within 0.83% of each other. However, for the S-shaped

Table 6. Values of voltage V_{rec} of 4MF using the WMS and the S-shaped coaxial cable over 2 days.

Point	WMS		S-shaped coaxial	
	Day 1 (V)	Day 2 (V)	Day 1 (V)	Day 2 (V)
1	53.12	53.03	57.98	59.05
2	45.53	45.18	48.91	50.35
3	53.36	53.18	58.88	57.83
4	45.13	45.06	49.55	47.98
5	53.03	52.97	56.28	57.25
6	44.98	44.78	48.18	46.75
7	52.88	52.27	57.63	55.78
8	45.17	45.03	48.71	49.16
9	36.05	35.82	39.66	37.81
10	36.18	36.02	40.05	41.11
11	30.31	29.91	32.94	33.53
12	36.21	36.45	41.13	38.55
13	36.35	36.04	41.87	39.01

cable, the measured values at points 1, 3, 5, and 7 are within 5.86%, and for points 9, 10, 12, and 13 are within 6.64%.

An additional experiment was done to show the mobility advantage of using the WMS versus the coaxial cables. This experiment was conducted using the 4MF configuration, a secondary load (R_L) of 10 k Ω , and 1.0 A (peak-to-peak) applied to the primary coil. We attached the WMS to a long plastic rod, connected to a stepper motor outside the cage, where the WMS was at point 11 in the cage. The motor was spaced 15 cm away from the cage. We then measured V_{rec} continuously from 0° to 360° (29 samples/s), to create the plot of V_{rec} versus orientation, as shown in Fig. 14. In contrast, using a coaxial cable to obtain such measurements while moving through a range of angles, would be difficult, due to mechanical stiffness, as well as continuous changes to the field caused by the cable (similar to different cable shapes as listed in Table 5). This demonstrates the mobility and orientation advantages of the WMS when measuring V_{rec} at any orientation with respect to the primary coil.

We also investigated our LCWPT behavior using different types of batteries to power the WMS. Since the WMS must provide reliable measurements over time, its power must be supplied independently (by a battery) to make its operation independent of the RID performance. We tested the use of

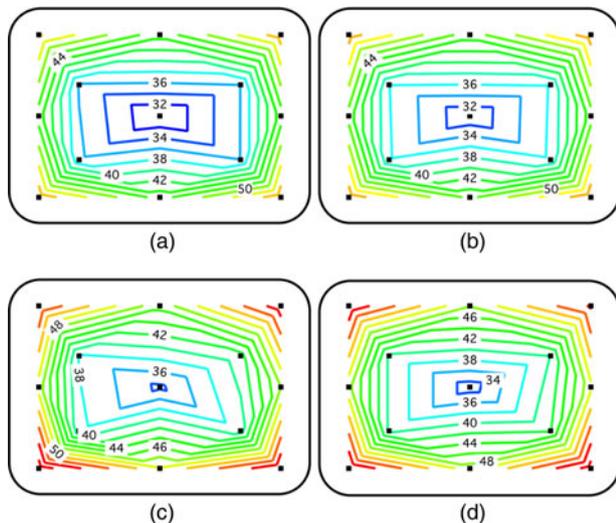


Fig. 13. Contour plot of the V_{rec} for the 13 points over 2 days; (a) Day 1 using the WMS, (b) Day 2 using the WMS, (c) Day 1 using the S-shaped coaxial cable and (d) Day 2 using the S-shaped coaxial cable.

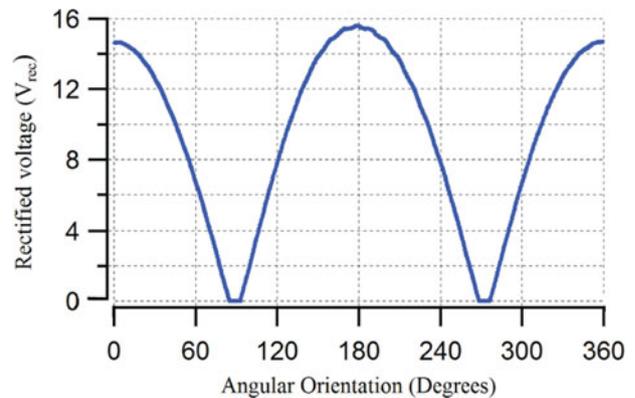


Fig. 14. Values of voltage V_{rec} of 4MF during continuous rotation at the center of the cage, versus orientations. Note the RID receives slightly more power while inverted, since it is not centered on the rod and thus changes both its angle and vertical position within the field.

AA, coin cell, and lithium-polymer batteries. The coin cell battery, or the lithium-polymer battery was placed in the field with the WMS. However, the AA battery was outside the cage, and connected to the WMS using twisted-pair wires. We found that the primary circuit draws more voltage and current from the DC supply when using the AA battery, or the coin cell battery, in comparison with the lithium-polymer battery. This is likely due to the metallic components of the AA or coin cell battery, which produce a load in the electromagnetic field. In addition, metallic objects near the field affect the inductance of the primary coil that leads to shifting of the operating point (resonant frequency) of the primary circuit [36]. The Class-E power amplifier compensates for the shift in resonant frequency, by drawing more DC current to maintain the sinusoidal current in the primary coil. The extra draw on the DC power supply was 0.1 A (1 V) using the coin cell batteries, and 0.3 A (2 V) using the AA batteries.

An additional note: the maximum power flows when the resistive load R_L is conjugately matched to the $L_S C_S$ tank circuit, as explained in [2]. Hence, our experimental measurements utilize a conjugately matched load (R_L) to ensure the maximum power transfer for the overall system. Each RID configuration has a different impedance magnitude (R_{LC}), as shown in Table 4. In order to determine the ideal resistor load (R_L) value for each RID, we tested resistor values of 1, 2.7, 5, 10, and 20 k Ω , to find the peak power transfer. For example, in the case of the *air core*, as shown in Fig. 15, we found that the R_L value of 5 k Ω provided best power transfer. Similarly, in the case of the 4MF configuration, the R_L value of 10 k Ω provided best power transfer. A Vector Impedance Meter was also used to verify the selected values.

VII. LCWPT EXPERIMENT RESULTS

Experiments to measure power transfer performance of the RID (*air core* and 4MF configurations) were conducted with the WMS. In these LCWPT experiments, the RID was located only at the center (point 11) of the cage. The experiments varied three independent parameters: the RID orientation (0° , 30° , 60° and 90° with respect to the x - y plane of the primary coil), the matched impedance of the secondary circuit, and the current (I_p) applied to the primary coil (1, 1.5, 2, and 2.5 A peak-to-peak sinusoidal). The resulting induced voltage V_{rec} in the RID was measured by the WMS.

A) Air core configuration

Figure 15 shows a plot of the power received by the *air core* configuration with different resistor loads, when the RID is located at the center of the primary coil, 3 cm above the cage floor, at a 0° orientation. The maximum power is found when using a matched load of 5 k Ω , where the maximum power is 58 mW with an applied primary coil current (I_p) of 2.5 A. Figure 16 shows the power received by the *air core* configuration with a matched load (5 k Ω) at 0° , 30° , 60° , and 90° orientations.

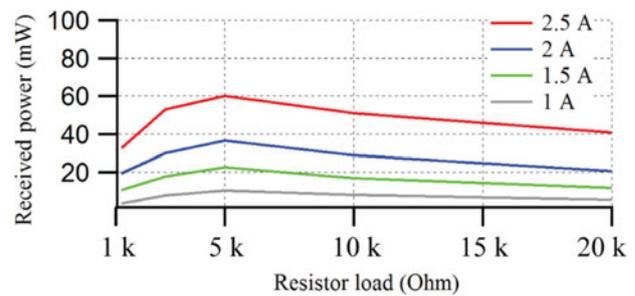


Fig. 15. Power received in the *air core* configuration versus resistor loads for different currents applied to the primary coil. The RID was located at the center of the primary coil, in a horizontal (0°) orientation.

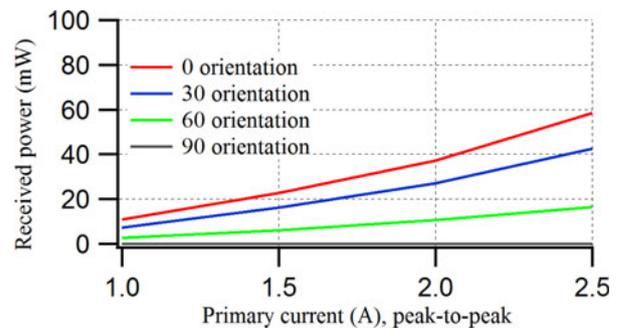


Fig. 16. Power received by the *air core*-based RID located at the center of the primary coil, with a 5 k Ω R_L .

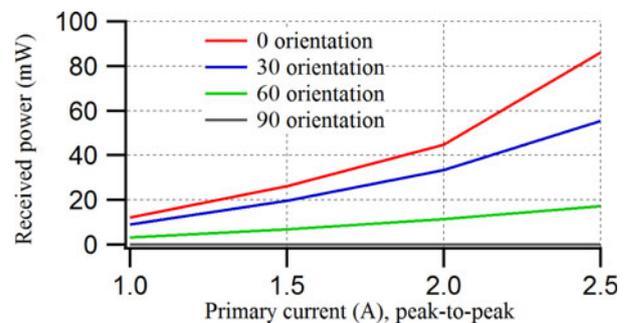


Fig. 17. Power received by the 4MF configuration at the center of the primary coil, with a 10 k Ω load R_L .

B) 4MF configuration

Figure 17 shows a plot of the power received by the 4MF configuration at the center of the primary coil. The 4MF configuration differs from the *air core* by the addition of four ferrite rods placed perpendicular to the PCB, as shown in Fig. 9 (b). The 4MF configuration required a R_L value of 10 k Ω , to ensure impedance matching within the RID. Addition of the ferrites improves the received power, where the maximum received power is 86 mW at a 0° orientation with an applied primary coil current (I_p) of 2.5 A. The ferrites also help the RID to gather power when it is tilted. For example, at an angle of 30° with respect to the horizontal plane, the 4MF can receive approximately the same power as the *air core* configuration at 0° . The 4MF configuration receives 1 mW at the 90° orientation.

VIII. DISCUSSION

The WMS collects performance data from the WPT system under test, and communicates the data wirelessly via radio link in real-time. The utility of the WMS is that it overcomes the problems that result when using directly connected coaxial cables or voltage/current probes to measure the secondary circuit. In our earlier work, we had measured the rectified voltage (V_{rec}) of the RID using various configurations of coaxial cables across the load (R_L , located outside the primary field); however, those measurements were plagued by offset and noise problems, and produced inconsistent results. When the same length of coaxial cable was bent in different shapes (with all other parameters fixed) the V_{rec} measurements varied by 5–27%, as shown in Table 5. This inspired the development of the WMS system presented in this paper. By using the WMS, the measurements of V_{rec} at various orientations and positions of the RID are consistent to within 0.5% from day-to-day as shown in Tables 5 and 6, whereas those from the coaxial cables varied by up to 7% from day-to-day. Hence, measurements using the WMS are more consistent and precise in comparison with coaxial cables.

Note that the WMS is not able to measure the induced AC voltage of the $L_S C_S$ tank circuit, because of a floating ground issue. This occurs since the measured voltage (V_M) over the voltage divider (Fig. 3) will be a floating signal with respect to the ADC of the microcontroller. The WMS was only designed to measure the rectified DC voltage (V_{rec}), as shown in Fig. 3.

When developing the WMS, we performed a rough check of the DC measurement accuracy. This was done by using a coaxial cable to measure the AC voltage directly across the $L_S C_S$ tank, even though we acknowledge the problems of Section VI and Table 5. We used a 5 k Ω (R_L) resistor at the opposite end of the coaxial cable (located outside the primary cage) and measured the induced voltage across R_L using a voltage probe connected to an oscilloscope. We found the induced AC voltage was 54.2 V (peak-to-peak) when driving the primary coil with (I_p) 2.5 A (peak-to-peak). An AC value of 54.2 V corresponds to a rectified voltage, V_{rec} , of 17.3 V DC, which approximately matches the measurements using the WMS, as shown in Table 5.

The power received by the RID is proportional to the square of the induced voltage (V_{ind}). Hence, the power transfer from primary to secondary of the WPT system can be increased by increasing the supply voltage (as long as the DC power supply is able to provide sufficient power, and V_{DS} across the MOSFET stays below the breakdown voltage). Therefore, the received power values in Figs 15–17 are relative to the primary current, and are intended to simply show the trends in comparison with system variables. The measure of a good WPT system is demonstrated by overall system efficiency [2]. We observed that the matched impedance of the *air core* configuration differs from that of the 4MF configuration. This is due to the lower quality factor and coupling coefficient of the *air core* compared with the 4MF configuration.

The overall weight of the RID and the WMS is 4.8 g, while the RID alone is less than 2 g. The WMS is not intended to be mounted on the head of a freely moving mouse, rather, only the RID (with an application circuit) is intended for a mouse. No animals were used in this study, where we have instead used fixtures and a rotating motor to approximate

some of the orientations that the RID would be in when attached to a freely moving mouse.

In general, the WMS system could also be used for performance measurement of various WPT systems. This could be done by modifying the configuration of the voltage dividers (R_1 and R_2) and by modifying R_3 and C_2 (filter), to allow the WMS to measure the induced DC voltage and the received power for any WPT application.

IX. CONCLUSION

This paper describes the design and testing of the WMS, which is designed to provide reliable measurements of LCWPT system performance during development of LCWPT systems. Our LCWPT system is used to transmit power to a telemetric recording device attached to a freely moving rodent. The WMS is battery powered, and transmits performance data by radio link, to avoid the measurement errors normally associated with cable-based measurement due to field interference, noise and offset. The WMS can measure rectified voltage (V_{rec}) values from 0 to 63 V, with 12-bit resolution, at 29 Hz, from the RID. Furthermore, the WMS was made to minimize its own interference with the resonance of the LCWPT system, and adheres to the design requirements summarized in Table 1 and parameters listed in Table 2. The WMS serves as a useful and portable tool to evaluate secondary circuit (RID) performance at various orientations and positions, without the problematic use of coaxial cables, or current/voltage probes within the primary field.

Physical prototypes of the WMS and RID configurations (*air core* and 4MF) were constructed. Experiments were done over a few days to demonstrate the repeatability of the WMS measurements (Tables 5 and 6), as well as experiments at various locations within the primary field (Figs 12 and 13). In addition, the versatility was shown by continuous data collection while the WMS was rotated by 360°, as shown in Fig. 14. The WMS does not significantly affect the electromagnetic field distribution of the primary coil, as shown by Figs 13(a) and 13(b), making it a valuable measurement tool. It also has little effect on the resonance of the LCWPT system, as noted by experiments with/without the WMS. These experimental results show that the WMS provides better measurement performance (consistency and precision) and versatility, in comparison with coaxial cable-based-measurement systems.

REFERENCES

- [1] Baker, M.W.; Sarpeshkar, R.: Feedback analysis and design of RF power links for low-power bionic systems. *IEEE Trans. Biomed. Circuits Syst.*, 1 (1) (2007), 28–38.
- [2] Badr, B.M.; Somogyi-Gsizmazia, R.; Delaney, K.R.; Dechev, N.: Wireless power transfer for telemetric devices with variable orientation, for small rodent behavior monitoring. *IEEE Sensors J.*, 15 (4) (2015), 2144–2156.
- [3] Kalialakis, C.; Georgiadis, A.: The regulatory framework for wireless power transfer systems. *Wireless Power Transf. J.*, 1 (2) (2014), 108–118.

- [4] Costanzo, A.; Dionigi, M.; Matri, F.; Mongiardo, M.; Russer, J.A.; Russer, P.: Rigorous network modeling of magnetic-resonant wireless power transfer. *Wireless Power Transf. J.*, **1** (1) (2014), 27–34.
- [5] Jow, U.; Ghovanloo, M.: Geometrical design of a scalable overlapping planar spiral coil array to generate a homogeneous magnetic field. *IEEE Trans. Magn.*, **49** (6) (2013), 2933–2945.
- [6] Pinuela, M.; Yates, D.C.; Lucyszyn, S.; Mitcheson, P.D.: Maximising DC-to-load efficiency for inductive power transfer. *IEEE Trans. Power Electron.*, **28** (5) (2013), 2437–2447.
- [7] Russel, D.; McCormick, D.; Taberner, A.; Lim, M.; Malpas, S.: Wireless power delivery system for mouse telemeter, in *IEEE BioCAS*, Beijing, China, November 26–28, 2009, 273–276.
- [8] Zhao, Y.; Nandra, M.; Yu, C.; Tai, Y.: High performance 3-coil wireless power transfer system for the 512-electrode epiretinal prosthesis, in *34th IEEE EMBS*, San Diego, USA, August 28–September 1, 2012, 6583–6586.
- [9] Xu, Q.; Wang, H.; Gao, Z.; Mao, Z.; He, J.; Sun, M.: A novel mat-based system for position-varying wireless power transfer to biomedical implants. *IEEE Trans. Magn.*, **49** (8) (2013), 4774–4779.
- [10] Xu, Q.; Gao, Z.; Wang, H.; He, J.; Mao, Z.H.; Sun, M.: Batteries not included: a mat-based wireless power transfer system for implantable medical devices as a moving target. *IEEE Microw. Mag.*, **14** (2) (2013), 63–72.
- [11] Dionigi, M.; Mongiardo, M.: A novel coaxial loop resonator for wireless power transfer. *Int. J. RF Microw.*, **22** (3) (2012), 345–352.
- [12] Dionigi, M.; Mongiardo, M.: Coaxial capacitor loop resonator for wireless power transfer systems, in *The 7th IEEE GeMiC*, Ilmenau, Germany, 2012, 1–4.
- [13] Yates, D.C.; Holmes, A.S.; Burdett, A.J.: Optimal transmission frequency for ultralow-power short-range radio links. *IEEE Trans. Circuits Syst.*, **51** (7) (2004), 1405–1413.
- [14] Abdolkhani, A.; Hu, A.P.: Magnetic coupling coefficient determination of IPT systems under operating conditions. *Wireless Power Transf. J.*, **1** (2) (2014), 83–86.
- [15] Yang, Z.; Liu, W.; Basham, E.: Inductor modeling in wireless links for implantable electronics. *IEEE Trans. Magn.*, **43** (10) (2007), 3851–3860.
- [16] Badr, B.M.; Somogyi-Csizmazia, R.; Delaney, K.R.; Dechev, N.: Maximizing wireless power transfer using ferrite rods within telemetric devices for rodents, in *COMSOL Conf.*, Boston, USA, October 7–9.
- [17] Tesla, N.: Apparatus for transmitting electrical energy. USA patent 1 119 732, December 1914.
- [18] Fotopoulou, K.; Flynn, B.W.: Wireless power transfer in loosely coupled links: coil misalignment model. *IEEE Trans. Magn.*, **47** (2) (2011), 416–430.
- [19] Moura, T.; Carvalho, N.B.D.; Pinho, P.: High-efficiency D-TV energy harvesting system for low-input power. *Wireless Power Transf. J.*, **3** (1) (2015), 34–42.
- [20] Microcontroller Nordic, nRF24LE1-F16Q48, ultra-low power wireless system, 2010.
- [21] Application note, RF design guidelines: PCB layout and circuit and circuit optimization. Available: www.semtech.com.
- [22] Application note, AN1294. Available: www.st.com.
- [23] Kim, J.-W.; Ryu, C.-K.; Han, Y.-O.: Development of SMD chip inductors for RF system applications. In *Convergence and Hybrid Information Technology* (eds: Lee, G.; Howard, D.; Ślęzak, D.; Hong, Y.S.), Springer-Verlag, Berlin, 2012, 602–610.
- [24] RF antenna “FR05-S1-N-0-110” (2015, July 16). [Online]. Available: http://www.fractus.com/sales_documents/FR05-S1-N-0-110/UM_FR05-S1-N-0-110.pdf.
- [25] Vandevoorde, G.; Puers, R.: Wireless energy transfer for stand-alone systems: a comparison between low and high power applicability. *Sensors Actuators* (eds: Huijsing, J.; Steyaert, M.; Roermund, A.V.), **92** (1–3) (2001), 305–311.
- [26] Sokal, N.O.; Sokal, A.D.: Class E-A new class of high-efficiency tuned single-ended switching power amplifiers. *IEEE J. Solid-State Circuits*, **10** (3) (1975), 168–176.
- [27] Lenaerts, B.; Puers, R.: *Omnidirectional Inductive Powering for Biomedical Implants*, Springer, Netherlands, 2009.
- [28] Gate driver “MIC4421” (May 16, 2015). [Online]. Available: <http://www.micrel.com>.
- [29] MOSFET “STP16NK65Z” (May 16, 2015). [Online]. Available: <http://www.st.com/>.
- [30] Sokal, N.O.; Sokal, A.D.: High-efficiency tuned switching power amplifier. USA Patent 3,919,656, 1975.
- [31] Sokal, N.O.: Class E high-efficiency switching-mode tuned power amplifier with only one inductor and one capacitor in load network-approximate analysis. *IEEE J. Solid-State Circuits*, **16** (4) (1981), 380–384.
- [32] Virili, M.; Georgiadis, A.; Collado, A.; Niotaki, K.; Mezzanotte, P.; Roslli, L.; Alimenti, F.; Carvalho, N.B.: Performance improvement of rectifiers for WPT exploiting thermal energy harvesting. *Wireless Power Transf. J.*, **2** (1) (2015), 22–31.
- [33] Rectifiers “NSDEM11XV6T1” (May 16, 2015). [Online]. Available: <http://www.onsemi.com/>.
- [34] Badr, B.M.; Somogyi-Csizmazia, R.; Dechev, N.; Delaney, K.R.: Power transfer via magnetic resonant coupling for implantable mice telemetry device, in *Proc. IEEE WPTC 2014*, Jeju, South Korea, May 8–9, 259–264.
- [35] Puers, R.; Schuylenbergh, K.V.; Catrysse, M.; Hermans, B.: Wireless inductive transfer of power and data. In *Analog Circuit Design*, Springer, Netherlands, ch. 18, 2006, 395–414.
- [36] Troyk, P.R.; Schwan, M.A.K.: Closed-loop class E transcutaneous power and data link for microImplants. *IEEE Trans. Biomed. Eng.*, **39** (6) (1992), 589–599.



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